# **3p-C-NETA-TATE:** A versatile somatostatin analogue for Al<sup>18</sup>F-labeled and therapeutic SSTR2 targeting radiopharmaceuticals



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#### Nuclear medicine:

Plays an important role in the diagnosis, follow-up and treatment of cancer

Radiopharmaceuticals consist mostly out of two parts:

Vector molecule with high affinity and selectivity for the target

→ Small organic molecule, peptide, antibody or antibody fragment

### 1) Radionuclide

→ Diagnostic radionuclide (PET or SPECT)  $\rightarrow$  Therapeutic radionuclide ( $\beta^2$ ,  $\alpha$  or Auger-electron emitters)

 $\rightarrow$  The radiopharmaceutical is distributed within the body by the vascular system and allows targeting of a primary tumor and all its metastases

### Target:

Low expression in healthy tissue

High expression in tumour tissue

 $\rightarrow$  Somatostatin receptors (SSTRs) are highly expressed in many neuroendocrine tumors (NETs)  $\rightarrow$  Excellent target for diagnosis and targeted radionuclide therapy (TRNT) of NETs

# Background

Somatostatin-based radiopharmaceuticals (e.g. [<sup>68</sup>Ga]Ga-DOTATATE and [<sup>177</sup>Lu]Lu-DOTATATE) have been used to diagnose, monitor, and treat neuroendocrine tumor patients with great success [1]. However, widespread implementation of [<sup>68</sup>Ga]Ga-DOTA-SSA PET in clinical practice is often hampered by practical, regulatory and economic factors related to <sup>68</sup>Ge/<sup>68</sup>Ga-generators, such as the high cost, limited availability, low activity yield per elution and regulatory and reimbursement barriers. The Al<sup>18</sup>F-method combines the advantages of a chelator-based radiolabeling method with the imaging and logistical advantages of fluorine-18. [<sup>18</sup>F]AIF-NOTA-octreotide, a promising <sup>18</sup>F-labeled somatostatin analogue and potential alternative for <sup>68</sup>Ga-DOTA-peptides, is under clinical evaluation [2].

A major drawback is that the most utilized chelator for the Al<sup>18</sup>F-method, 1,4,7triazacyclononane-N,N',N''-triacetic acid (NOTA), is not compatible with therapeutic radionuclides such as the  $\beta$ --emitter lutetium-177 (<sup>177</sup>Lu) and the promising  $\alpha$ -emitter bismuth-213 (<sup>213</sup>Bi). Ideally, the same precursor (combination of chelator-linker-vector) can be used for production of both diagnostic and therapeutic radioprobes with very similar (e.g. Al<sup>18</sup>F/<sup>213</sup>Bi/<sup>177</sup>Lu) pharmacokinetic properties, which is possible with the promising chelator 3p-C-NETA (Figure 1) [3], allowing accurate personalised dosimetry estimation, and radionuclide therapy of NET patients in a theranostic setting.

In contrast to external high energy photon or proton therapy, targeted radionuclide therapy (TRNT) is a systemic cancer treatment allowing targeted irradiation of a primary tumor and all its metastases, resulting in less collateral damage to normal tissues. The single  $\alpha$ -emitting radionuclide <sup>213</sup>Bi (T<sub>1/2</sub> = 45.6 min, E $\alpha$  = 8.4 MeV,  $\gamma$  = 440 keV,  $\alpha$ -particle range = 40–80  $\mu$ m, corresponding to 2-10 cell diameter) has interesting properties and might be considered as a magic bullet for TRNT [4]. Further, it can be produced on site using a <sup>225</sup>Ac/<sup>213</sup>Bi generator.



Figure 1. Versatility of 3p-C-NETA in contrast to NOTA. (A): NOTA is only suitable for radiolabeling of diagnostic radionuclides (Al18F and 68Ga). (B): In contrast, 3p-C-NETA has potential for both diagnostic (Al<sup>18</sup>F) and therapeutic radionuclides (<sup>213</sup>Bi, <sup>177</sup>Lu, and <sup>161</sup>Tb), making it a true theranostic chelator.

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**Objectives** 

In this study we evaluated 3p-C-NETA-TATE as theranostic precursor for NET imaging and therapy, and present first results of the preclinical evaluation of the diagnostic compound [<sup>18</sup>F]AIF-3p-C-NETA-TATE [5] and therapeutic ligands [<sup>213</sup>Bi]Bi-3p-C-NETA-TATE and [<sup>177</sup>Lu]Lu-3p-C-NETA-TATE.

# **Materials and Methods**

3p-C-NETA-TATE was synthesized using standard solid/liquid-phase peptide synthesis and purified using HPLC. [<sup>18</sup>F]AIF-3p-C-NETA-TATE was synthesized in an automated AllinOne® synthesis module. 3p-C-NETA-TATE (10  $\mu$ M) was radiolabeled manually with <sup>177</sup>Lu (NaOAc, 0.1 M, pH 4.1, 12 min) or <sup>213</sup>Bi (Tris-HCl, 4 M, pH 8.5, 7 min) at 40 or 95 °C. The *in vitro* stability of the corresponding radiocomplexes was evaluated in formulation buffer, PBS and human serum at 37 °C using radioHPLC.

In vitro cell binding and internalization was performed for [<sup>18</sup>F]AIF-3p-C-NETA-TATE, [<sup>213</sup>Bi]Bi-3p-C-NETA-TATE (185 kBq/well; A<sub>m</sub>: 1.23 GBq/µmol) and [<sup>177</sup>Lu]Lu-3p-C-NETA-TATE (53 kBq/well; 176.66 A<sub>m</sub>: GBq/μmol) using SSTR2 expressing cells (QGP1.SSTR2 and/or BON1.SSTR2) [4] and the pharmacokinetics of [<sup>18</sup>F]AIF-3p-C-NETA-TATE were evaluated in healthy rats and in xenograft (QGP1.SSTR2) bearing mice using  $\mu$ PET/MRI and  $\mu$ PET/CT, respectively. [<sup>18</sup>F]AIF-NOTA-Octreotide was used as benchmark. Cell viability and clonogenic assays were performed with [<sup>213</sup>Bi]Bi-3p-C-NETA-TATE and [<sup>177</sup>Lu]Lu-3p-C-NETA-TATE using BON.SSTR2 cells.

[<sup>18</sup>F]AIF 3p-C-NETA-TATE was obtained in good RCY (56 ± 10%) and >98% radiochemical purity. [<sup>18</sup>F]AIF-3p-C-NETA-TATE displayed excellent in vitro stability with >95% intact tracer after 4 hours in all tested conditions. High SSTR2 specific cell binding and internalization (18.4 ± 2.1 % of which 78.3 ± 2.1 % is internalized) was observed after 60 min incubation (Figure 2). Finally, [<sup>18</sup>F]AIF-3p-C-NETA-TATE showed excellent pharmacokinetic properties (rats and mice) and tumor accumulation (SUV<sub>mean</sub>60 min:2.7 ± 1.1), which was comparable as for  $[^{18}F]AIF-NOTA-Octreotide (SUV_{mean} 60 min:3.2 \pm 0.76)$ . We were also able to block uptake in SSTR2 expressing organs and in tumors (>90%) by coinjection of 2.5 mg/kg octreotide acetate, indicating SSTR2 specific uptake (Figure 3 and 4). 3p-C-NETA-TATE efficiently sequestered <sup>177</sup>Lu (RCC >95%) and <sup>213</sup>Bi (RCC >90%) at 12 and 7 min respectively at 40 °C (Figure 5). [<sup>177</sup>Lu]Lu-3p-C-NETA-TATE showed excellent in vitro stability in both PBS and mouse serum ( >90% intact complex at day 3). Starting with 94.3% radiochemical purity, [<sup>213</sup>Bi]Bi-3p-C-NETA-TATE demonstrated good stability (>90% intact radiocomplex) after 5 h in both PBS and human serum. High SSTR2 specific cell binding and internalization (11.4  $\pm$  0.7 % of which 62.1% is internalized) was observed after 60 min incubation for  $[^{177}Lu]Lu-3p-C-NETA-TATE$  whereas only 3.3 ± 0.5% cell binding (of which 39.2% is internalized) was observed for [<sup>213</sup>Bi]Bi-3p-C-NETA-TATE, probably due to blocking effects because of low apparent molar activity. >99% blocking after co-incubation with 100 μM octreotide was observed for both tracers at 60 min (Figure 6). Reduced viability of BON-1.SSTR2 was observed after 48 h incubation with  $[^{213}Bi]Bi-3p-C-NETA-TATE$  (9.9 ± 0.9% viability at 0.1 MBq activity). Also, only 0.1 MBq activity of [<sup>213</sup>Bi]Bi-3p-C-NETA-TATE was required to achieve cell surviving fraction of 0.1 (SF<sub>0.1</sub>).

# Results



*Figure 2*. Cell binding and internalization of [<sup>18</sup>F]AIF-3p-C-NETA-TATE on BON1.SSTR2 and QGP1.SSTR2 cell lines. Adherent cells were incubated with the radioligand of interest (n = 3, 180-190 kBq/well) for 5, 10, 30, 60, 120, 180 and 240 min at 37 °C in the presence or absence of octreotide acetate (100  $\mu$ M, n = 3). Total bound fraction is the sum of membrane bound + internalized fraction.



Figure 3. In vivo biodistribution of [18F]AIF-3p-C-NETA-TATE in rats using control and blocking conditions (2.5mg/kg octreotide). A,D) Maximum intensity projections (PET) at 65-75 minutes post-injection, with SSTR2-expressing organs (pituitary and adrenal glands, pancreas) highlighted by arrows in representative naïve (top) and blocked (bottom) animals. **B,E)** Time activity curves (TACs) of SSTR2-expressing organs in naïve (top) and blocked (bottom) animals (n=3), demonstrating high and blockable SSTR2 uptake. **C,F)** Coronal slices indicating delineation of adrenal glands on MRI sequence subsequently applied to PET data to generate TAC. (upper): PET-MRI fusion, (middle): PET (lower): MRI (PET images from 65-75 min timepoint).

### References



3p-C-NETA-TATE is an excellent and versatile agent that can be used for both targeted radionuclide therapy (<sup>177</sup>Lu, <sup>213</sup>Bi) and diagnostic applications (Al<sup>18</sup>F) and has advantages as an alternative to the DOTA-SSA analogues in current clinical use. [<sup>18</sup>F]AIF-3p-C-NETA-TATE and [<sup>213</sup>Bi]Bi-3p-C-NETA-TATE/[<sup>177</sup>Lu]Lu-3p-C-NETA-TATE will be further evaluated as potential theranostic pairs in SSTR2 expressing tumor mice.



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*Figure 5.* Radiochemical conversions (RCC) of [<sup>177</sup>Lu]Lu-3p-C-NETA-TATE and [<sup>177</sup>Lu]Lu-DOTA-TATE. 3p-C-NETA-TATE (0.1-20  $\mu$ M) or DOTA-TATE (0.1-20  $\mu$ M) was labeled with 2-5 MBq of [<sup>177</sup>Lu]LuCl<sub>3</sub> (0.4 M NaOAc, pH 4.1) for 15 min at 40, 60 or 95 °C. Blue line is inserted to indicate a yield of 95%;



Figure 6. Cell binding and internalization of on BON1.SSTR2 cell lines. Adherent cells were incubated with the radioligand of interest (n = 3, 180-190 kBq/well) for 5, 10, 30, 60, 120, 180 and 240 min at 37 °C in the presence or absence of octreotide acetate (100  $\mu$ M, n = 3). Bound fraction is the sum of membrane bound + internalized fraction.

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# Conclusions

*Figure 4.* μPET imaging of [<sup>18</sup>F]AIF-3p-C-NETA-TATE in QGP1.SSTR2 tumor bearing mice. MIP image (65–75 min p.i.): (left) [<sup>18</sup>F]AIF-3p-C-NETA-TATE; (right) [<sup>18</sup>F]AIF-3p-C-NETA-TATE + 5 mg/kg octreotide. Blue circle and black arrow indicate tumor and thymus region



## **Acknowledgements and contact**